



A virtual reality bus ride as an ecologically valid assessment of balance: a feasibility study

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Abstract

Balance disorders can have substantial adverse implications on the performance of daily activities and lead to an increased risk of falls, which often have severe negative consequences for older adults. Quantitative assessment through computerized force plate-based posturography enables objective assessment of postural control but could not successfully represent specific abilities required during daily activities. The use of virtual reality (VR) could improve the representative design of functional activities and increase the ecological validity of posturographic tests, which would enhance the transferability of results to the real world. In this work, we investigate the feasibility of a simulated bus ride experienced in a surround-screen VR system to assess balance with increased ecological validity. Participants were first evaluated with a posturography test and then with the VR-based bus ride test, while the reactions of their centre of pressure were registered. Lastly, participants provided self-reported measures of the elicited sense of presence during the test. A total of 16 healthy young adults completed the study. Results showed that the simulation could elicit significant medial–lateral excursions of the centre of pressure in response to variations in the optical flow. Furthermore, these responses' amplitude negatively correlated with the participants' posturography excursions when fixating a target. Although the sense of presence was moderate, likely due to the passive nature of the test, the results support the feasibility of our proposed paradigm, based in the context of a meaningful daily living activity, in assessing balance control components.

Keywords Virtual reality · Balance assessment · Posturography · Ecological validity · Visual motion

1 Introduction

The ability to move upright while maintaining balance has attracted the attention of researchers in different areas, from sports applications to rehabilitation of neuromuscular diseases. Balance disorders or problems maintaining postural balance can have substantial implications on the performance of most daily activities and lead to an increased risk of falls (Salzman 2010), which often have severe consequences for older adults. In the elderly population, these disorders and the resulting falls are a significant cause of long-term functional impairments, disability, injury, mortality, and loss of independence and quality of life (Rubenstein 2006; Salzman 2010). Because balance disorders are common in many neurological diseases, such as Parkinson's Disease, Stroke, and Multiple Sclerosis, their accurate assessment is essential to plan effective rehabilitation treatments (Claesson et al. 2017; Mihara et al. 2012).

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41 Clinical assessment tools allow for qualitative functional
 42 assessment of balance deficits and risk of falls. However,
 43 many qualitative tests rely on coarse and subjective rating
 44 scales, partial to tester bias, to measure a complex motor
 45 behaviour (Mancini and Horak 2010). A system-level
 46 approach is needed to identify the fundamental causes of
 47 balance deficits and prescribe specific treatment (Mancini
 48 and Horak 2010). As balance control is derived from multi-
 49 sensory integration of somatosensory, visual, and vestibular
 50 systems, different tests exist, such as the Balance Evalua-
 51 tion Systems Test or the Physiological Balance Profile,
 52 which aim to assess each subsystem separately and during
 53 intersensory conflicts. The Balance Evaluation Systems Test
 54 (Horak et al. 2009) aims to identify which of 6 biomechanical
 55 and neural mechanisms of balance control are deficient
 56 so that proper rehabilitation can be designed. The Physi-
 57 ological Balance Profile (Lord and Clark 1996) measures
 58 five physiological functions to discriminate between fallers
 59 and non-fallers. Objective quantitative assessment through
 60 computerized, force plate-based, static posturography offers
 61 an alternative way to perform balance assessment without
 62 some of its drawbacks: variability within and across testers,
 63 the subjectivity of the scoring system, and insensitivity to
 64 small changes (Mancini and Horak 2010; Tyson and Con-
 65 nell 2009). Dynamic posturography introduces controlled
 66 perturbations to selectively manipulate a sensory input
 67 of balance control, such as optical flow/vection (Mancini
 68 and Horak 2010). However, for community-dwelling older
 69 adults, most of the research-based assessments are abstract
 70 single-tasks evaluations that do not feature a representa-
 71 tive design of functional activities and underrepresent their
 72 demands. Furthermore, it is understood that balance training
 73 is task specific and does not transfers to tasks with different
 74 demands, resulting in its performance increases not being
 75 correctly assessed by generic balance tests (Elion et al. 2015;
 76 Giboin et al. 2015; Naumann et al. 2015). Consequently,
 77 there is a need for instruments that better reflect postural
 78 control demands in daily-life situations (Pardasaney et al.
 79 2013). If "*ecological validity refers to the extent to which*
 80 *the environment experienced by the subject in a scientific*
 81 *investigation has the properties it is supposed or assumed*
 82 *to have by the investigator"* (Bronfenbrenner 1977), most
 83 of these assessments lack ecological validity, which could

hinder their transferability to the real world.

85 Advances in Information and communications technolo-
 86 gies—ICT, namely in software and hardware, have led to the
 87 easy access to technologies that were up to recent years con-
 88 strained to high-end laboratories and clinics, such as force
 89 plates, virtual reality (VR) systems, and physiological com-
 90 puting systems. As discussed previously, force plate-based
 91 posturography is an advantageous instrument in the assess-
 92 ment of balance, but its high cost and space requirements
 93 are a limitation to their general adoption (Visser et al. 2008).

94 Meanwhile, the low-cost Wii Balance Board (WBB) (Nin-
 95 tendo Co., Ltd., Kyoto, Japan), designed as a console game
 96 controller, has reported being similar to laboratory-grade
 97 force plates in validity and reliability (Clark et al. 2010;
 98 Huurnink et al. 2013). For that reason, posturography sys-
 99 tems that use the WBB as a low-cost force plate have been
 100 proposed and studied (Clark et al. 2011, 2010; Huurnink
 101 et al. 2013; Llorens et al. 2016).

102 VR simulations provide real-world-like experiences (Ber-
 103 múdez i Badia et al. 2016; Burdea and Coiffet 2003; Jerald
 104 2015), a realism that is brought by the immersive charac-
 105 teristics of the system (Bowman and McMahan 2007) and
 106 subjectively felt by the participants as *presence*, or the sense
 107 of *being there* (Jerald 2015). Immersion is the set of objec-
 108 tive characteristics of a VR system regarding which senses it
 109 extends to, which ones are disconnected from reality (inclu-
 110 sive), how surrounding are the stimulus, the vividness of
 111 information, the match between proprioception and virtual
 112 information, and self-representation (Slater et al. 1996;
 113 Slater and Wilbur 1997). In contrast, presence is a subjective
 114 feeling of participants when experiencing VR, modulated
 115 by the system, the content of the virtual environment (VE),
 116 and the participant's personal traits. The manipulation of
 117 the participants' sense of reality during a VR simulation
 118 to match the real environment's properties potentially adds
 119 to the ecological validity of an experiment and could take
 120 us a step closer to the real scenario without its main draw-
 121 back, lack of control. VR systems of different natures have
 122 their advantages. Surround-screen systems such as CAVEs
 123 (Cruz-Neira et al. 1992) have large fields-of-view, require
 124 limited or no wearable technology, and provide full-body
 125 tracking and self-representation (Gonçalves and Bermúdez
 126 2018). While modern occlusive Head-Mounted-Displays
 127 (HMD) are visually inclusive and completely surrounding
 128 in field-of-regard, they can influence motion and posture
 129 due to their added weight to the head (Morel et al. 2015)
 130 and have a higher chance of producing dizziness and cyber-
 131 sickness due to head rotation latency (Sherman and Craig
 132 2018). Notwithstanding, VR has been shown to be able to
 133 provide standardized, reproducible, and controlled VEs for
 134 the assessment of balance (Morel et al. 2015).

135 In an effort to design an objective and ecologically valid
 136 assessment test that could overcome the limitation in the
 137 transferability of posturographic results to real-world situa-
 138 tions, we developed the "VR Bus Assessment of Balance".
 139 The test combines the objective assessment of postural
 140 adjustments through measures of the centre of pressure, as
 141 in standardized posturographic tests, with sensory stimula-
 142 tion through the recreation of a realistic, meaningful task
 143 in an immersive environment, as in VR applications. Our
 144 proposed system consists of dedicated software and is imple-
 145 mented on a low-cost VR surround-screen projection system
 146 of high immersive characteristics, which can successfully

147 induce presence (Gonçalves et al., n.d.; Gonçalves and Bermúdez 2018). The system is instrumented with a Kinect v2
 148 (Microsoft Corp., Redmond, Washington, USA.), a WBB,
 149 and Plux BioSignals (PLUX wireless biosignals S.A., Lis-
 150 bon, Portugal), and allows the analysis of motion, postural
 151 control, electrocardiography, electromyography and elec-
 152 trodermal activity. The VR Bus Assessment of Balance
 153 visually simulates a bus ride through the streets of a city,
 154 where the participant acts as a standing passenger and is
 155 required to maintain balance. By simulating a bus ride, the
 156 user is exposed to controlled manipulations of optical flow
 157 in a meaningful everyday activity, increasing the ecological
 158 validity of the assessment, and, potentially, the transfer of
 159 results to real-world situations. While, in terms of ecological
 160 validity, this system lacks motion (moving or tilting), hap-
 161 tics, and stimulation of the participant's vestibular system,
 162 it compensates it with its simplicity, low-cost devices and
 163 safety, which substantially reduces the existing barriers for
 164 clinical acceptance and deployment of such an approach.
 165 Additionally, not only visual input plays an important role
 166 in balance and postural control in the general population bus
 167 is of particular importance post-stroke (Bonan et al. 2004;
 168 Yelnik et al. 2006; Navalón et al. 2014).

169 In this work, we investigate the feasibility of the VR Bus
 170 Assessment of Balance to assess healthy young adults' bal-
 171 ance performance by comparing its results with a validated
 172 WBB-based posturography balance assessment battery
 173 (Llorens et al. 2016). First, we measure the extent to which
 174 participants felt present in the simulated world, which could
 175 support the tool's ecological validity. Second, we investigate
 176 if this tool can produce observable and significant changes in
 177 participants' posture, measured through reactions of the centre
 178 of pressure (CoP) to variations in the optical flow. Lastly,
 179 we examine possible correlations between the participants'
 180 responses to the simulated optical flow and their individual
 181 ability to keep balance.
 182

183 2 Methods

184 2.1 Application and VR system

185 The VR Bus Assessment of Balance was built with the game
 186 engine Unity 3D (Unity Technologies, San Francisco, USA).
 187 The ride's backdrop is the virtual streets of Reh@City, a
 188 grid plan neighbourhood of a city with over 200 buildings,
 189 some parks, and other vehicles (Paulino et al. 2019). Reh@
 190 City also features billboards and storefronts of real brands
 191 and businesses familiar to the study participants, aiming to
 192 further increase the ecological validity of the experience.
 193 Also, with this aim, the interior of the virtual bus was mod-
 194 elled to resemble a bus of the local urban bus service. The
 195 bus ride drives a closed circuit at speeds ranging from 5.7

196 to 32 km/h. It undergoes several accelerations and decelera-
 197 tions of around 1.5 m/s^2 (0.15 g) and brief breaks of 4.7 m/s^2
 198 (0.45 g). The circuit has nine left turns, and five right turns,
 199 with a peak angular velocity from 13 to $16^\circ/\text{s}$, and it takes
 200 approximately 4.5 min to complete (Fig. 1). The sound of the
 201 Bus engine and passing cars is implemented coherently
 202 with the simulation behaviour.

203 The experience takes place inside a CAVE, comprising
 204 a low-cost VR monoscopic surround-screen projection sys-
 205 tem of high immersive characteristics, mediated through
 206 the KAVE software (Gonçalves and Bermúdez 2018). The
 207 display consists of the front projection into the three inside
 208 walls and floor of a cube-like structure, where each wall is
 209 2.8 m wide by 2.1 m tall, and the pixel density is approxi-
 210 mately 4 pixels per cm. The system uses a Kinect v2 to track
 211 the user's head and adapt the immersive projection on the
 212 walls and floor to its position in real time. It also features a
 213 5.1 surround sound system.

214 During the virtual ride, data are collected synchronously
 215 at 30 Hz from the virtual bus itself (position and orienta-
 216 tion), from a WBB (CoP position over the board), and the
 217 Kinect v2 sensor (3-dimensional position of the 25 joints'
 218 skeleton). The VR application, together with the system
 219 used, and the local bus's interior, are shown in Fig. 2.

220 2.2 WBB-based posturography system

221 A WBB-based posturography system, previously validated
 222 with 144 healthy adults and 53 individuals with stroke (Llorens
 223 et al. 2016), was used in this study to provide a reference
 224 assessment of balance. The system includes three standard-
 225 ized assessment protocols, the modified Clinical Test of
 226 Sensory Interaction on Balance (mCTSIB), the Limits of
 227 Stability (LOS), and the Rhythmic Weight Shift (RWS). The
 228 mCTSIB measures mean speed and maximum excursion of
 229 CoP in the medial-lateral and anterior-posterior axes for
 230 30 s in 4 conditions, eyes open and closed over a flat sur-
 231 face, and eyes open and closed over foam, to detect sensory
 232 impairments during quiet stance. The LOS measures the
 233 maximum controlled CoP excursion in 8 directions without
 234 losing balance. Lastly, the RWS measures the directional
 235 control of participants' CoP when rhythmically following a
 236 visual reference in both the medial-lateral and anterior-pos-
 237 terior axes.

238 2.3 Participants

239 A convenient sample of participants was recruited from
 240 the body of researchers of a research institute. The inclu-
 241 sion criteria were to be 18 years old or older, understand
 242 English, no known balance-related injuries or surgery, and
 243 no motor or cognitive limitations or epilepsy. A total of 18
 244 people volunteered to participate. The first participant was



Fig. 1 Top view of Reh@city with the bus route in yellow

Fig. 2 Interior of a local bus and the VR Bus Assessment of Balance underway



245 used to test and rehearse the protocol, and another one failed
 246 to follow the instructions during the experiment; therefore,
 247 their data were not included for analysis. Sixteen partici-
 248 pants, nine women, and seven men, with an average age of
 249 31.3 ± 6.5 years, a weight of 65.53 ± 11.85 kg, and a height
 250 of 1.69 ± 0.08 m, completed the study.

251 2.4 Procedure

252 Participants performed the experiment individually. First,
 253 they were introduced to the experiment, the procedure,
 254 and were answered any questions they had; then, they pro-
 255 vided their written informed consent. A characterization

questionnaire followed this. Their balance and postural 256
 control were assessed with the WBB-based posturography 257
 system, and a short rest of 2 min followed. Next, they were 258
 introduced to the VR surround-screen projection system. 259
 Participants were positioned barefoot over the WBB, facing 260
 the front wall, 2 m away from it, and aligned with its centre 261
 (Fig. 3). They were instructed not to move their feet and keep 262
 the arms along the body, other than that they were asked to 263
 act as a standing bus passenger over the WBB and were free 264
 to look around. After those instructions, they completed the 265
 VR bus ride. Lastly, participants were asked to rate their 266
 sickness and dizziness on a 1–7 Likert scale and answered 267
 the 3-item Slater-Usoh-Steed Questionnaire (SUS) (Slater 268

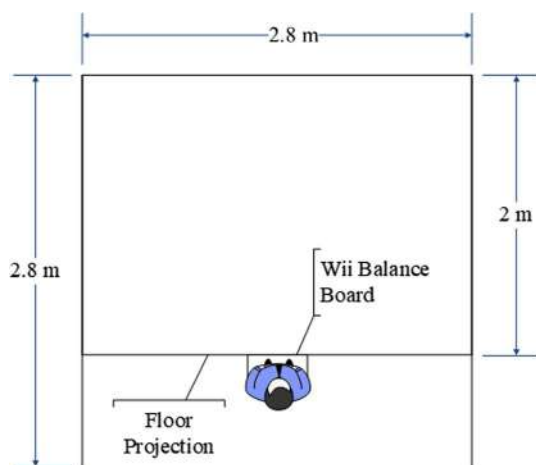


Fig. 3 Top view of the VR system projection surfaces with WBB and participant placement

et al. 1995), and the Presence Questionnaire (PQ), including 19 core items and 3 audio items (Witmer et al. 2005; Witmer and Singer 1998).

2.5 Analysis

Data were analysed in three ways, each corresponding to one of the goals stated in the introduction. First, we report descriptive statistics of the results from the questionnaires regarding presence and cybersickness. Second, the time-series data for each participant experiment were reduced to segments of interest that fitted into 3 types of events, according to the bus trajectory and speed: straight trajectory at constant speed, straight trajectory with speed changes, and turns. For each of the events, three posturography measures were calculated from the WBB CoP position: maximum excursion in the medial–lateral axis, maximum excursion in the anterior–posterior axis, and mean speed. Due to the non-normal distribution of the data, nonparametric tests were used. The Kruskal–Wallis test was used to find if the type of trajectory had a significant

effect on the three measures. The Mann–Whitney test with Bonferroni correction was used to follow up on these findings and understand between which pair of trajectory types those differences were significant. Second, for each participant, the same three measures were averaged for events of the same type, to get the participant’s average CoP behaviour for straights, speed changes, and turns. Lastly, the correlation between these values and metrics obtained from the posturography evaluation was calculated for each type of event. The significance level used was $\alpha = 0.05$ in all the analyses, and Bonferroni’s correction was used to correct for multiple comparisons. The analysis was done using IBM SPSS Statistics 22 (IBM, New York, USA) and MatLab 2013b (MathWorks, Massachusetts, USA).

3 Results

3.1 Subjective evaluation of the VR bus ride

The two questionnaires used to measure the subjective feel of presence experienced by participants evidenced moderate levels of presence reported, as described by a score of 50.72% [3–21] in the SUS and 65.74% [19–133] in the PQ. Individual analysis of the items of the PQ showed that participants rated the interface (projections and Kinect) and sounds of the VR Bus Ride with scores of 88.56% and 78.11% [3–21], respectively, which support the high immersion provided by the system. According to the self-evaluation of performance, rated with 75.5% [2–14], participants found it easy to adapt to the experience. In contrast, factors related to interaction with the virtual environment received lower scores, with the possibilities to act and examine having the lowest scores, being 52.3% [4–28] and 66.3% [3–21]. With a score of 60.57% [7–49], the realism of the experience was found to be moderate and slightly lower than the overall presence score. Finally, the levels of sickness or dizziness reported after the experiment were very low (Table 1).

Table 1 Descriptive statistical values of the subjective evaluation of the VR Bus Ride experience

Variable	[Range]	Mean \pm SD	% of range
Presence SUS	[3–21]	12.13 \pm 3.81	50.72% \pm 21.17%
Presence Q. (core 19-items)	[19–133]	93.94 \pm 19.13	65.74% \pm 16.78%
Realism	[7–49]	32.44 \pm 9.22	60.57% \pm 21.95%
Possibility to act	[4–28]	16.56 \pm 6.40	52.33% \pm 26.67%
Quality of interface	[3–21]	18.94 \pm 2.14	88.56% \pm 11.89%
Possibility to examine	[3–21]	14.94 \pm 3.09	66.33% \pm 17.17%
Self-evaluation of performance	[2–14]	11.06 \pm 2.79	75.50% \pm 23.25%
Sounds (3-items, not core)	[3–21]	17.06 \pm 3.64	78.11% \pm 20.22%
Sickness	[1–7]	1.69 \pm 1.54	11.50% \pm 25.67%
Dizziness	[1–7]	1.88 \pm 1.26	14.67% \pm 21.00%

3.2 Responses of the centre of pressure during the VR bus ride

The maximum excursion of the CoP in the medial–lateral axis and mean speed were significantly affected by the type of bus trajectory, $H(2)=21.99$, $p < 0.05$ and $H(2)=79.46$, $p < 0.05$, respectively. In contrast, the bus trajectory did not influence the maximum excursion in the anterior–posterior axis $H(2)=3.42$, $p=0.181$. A pairwise comparison of the three road events for the two affected metrics showed that both had significantly ($p < 0.0083$) lower values in the straight trajectory segments of constant speed than during the turns, $U=4904$ and $U=4891$. Again, both had significantly ($p < 0.0083$) lower values in straight segments with speed changes than in turns, $U=39,310$ and $U=27,900$. Neither measure showed differences between straight trajectories of constant speed and straight speed changes, $U=12,057$, $p=0.099$ and $U=12,369$, $p=0.174$. The bus turns, then, significantly increased maximum CoP excursion in the medial–lateral axis and mean speed, compared to straight trajectories, independently of the acceleration.

3.3 Relation of responses of the centre of pressure during VR bus ride and balance measures

The maximum excursion in the medial–lateral axis and mean speed of the participant's CoP during bus turns significantly correlated ($p < 0.05$) with the measures during the eyes-open condition of the mCTSIB. As seen in Table 2, participants with higher medial–lateral excursions in reaction to the bus's virtual turns had a lower maximum excursion when fixating a static target during the posturography assessment. The same was true for straight trajectories with velocity changes. Neither the maximum excursion (in both axis) nor the mean speed of the participant's CoP during straight bus trajectories of constant speed correlated with any relevant metrics assessed by the mCTSIB.

Table 2 Significant correlations between responses of the centre of pressure during the VR Bus Ride and the modified clinical test of sensory interaction on balance

		Eyes-open condition of the mCTSIB		
		Max. Exc. Ant-Post	Max. Exc. Med-Lat	Mean Speed
VR Bus Ride	Turns	ns	ns	ns
	Max. Exc. Med-Lat	-.695	-.523	ns
	Mean Speed	ns	ns	.520
Straight trajectories with speed changes	Max. Exc. Ant-Post	ns	ns	ns
	Max. Exc. Med-Lat	-.641	-.557	ns
	Mean Speed	ns	ns	ns

ns non-significant

4 Discussion and conclusions

This work evaluated the feasibility of using an immersive simulation of a bus ride, from a passenger perspective, to assess balance and postural control from an ecological valid standpoint. We started by evaluating how much the participants felt present in the simulation and not in a laboratory. Then, we tested if different behaviours of the bus during the visual simulation would produce observable effects on participants' posture. Finally, we explored the relationship between the participants' postural responses to the visual simulation and their posturography results from a validated tool.

Following previous investigations of balance, a surround-screen system was used instead of an HMD to avoid wearing a device on the head, which has been shown to impact balance (Morel et al. 2015), and preserves direct visual feedback of the participants' body. Furthermore, it induces much lower levels of cybersickness, due to lower apparent latency to head rotation (Sherman and Craig 2018); this also helps to mitigate what would be otherwise an uncontrolled element in the simulation. This was confirmed by our results, with participants reporting almost residual levels of sickness and dizziness.

Regarding the examination of the ecological validity of the test through the elicited sense of presence, reports to the SUS in our study were lower than previous experiments performed by the authors in a VR search task with the same system. However, the results from the PQ are much more in line with previous studies' results and even higher than some (Borrego et al. 2016; Gonçalves et al., n.d.). High results for "quality of the interface" and "sounds" indicate that participants valued the system's immersive characteristics and the quality of the three interfacing elements, i.e. visual and audio feedback, and input. However, the Kinect's perspective control was not noticeable, as the bus test required to remain static. Therefore, interpretation of the ratings to the "quality of the interface" might not be obvious. Participants

393 also reported high values of self-evaluation of performance,
 394 considering the system easy and quick to adapt to. Again,
 395 considering the passive and static nature of the experience,
 396 it was expected that both the possibilities to act and examine
 397 would have low values, which was indeed the case. Finally,
 398 the realism score evidences that maintaining static balance
 399 during a real bus ride encompasses multiple and complex
 400 perturbances that challenge human balance, which were
 401 not considered in the VR simulation. As mentioned in the
 402 introduction, balance training has been shown to be task-
 403 specific, not transferring to other tasks with different pos-
 404 tural demands, and individual balance abilities to be mostly
 405 experience and task-dependent. This can lead to the failure
 406 of generic balance tests to assess their outcomes and not
 407 address the specific postural demands of functional activities
 408 of daily living. This knowledge should drive efforts to use
 409 more ecologically valid assessments. Resulting in the proper
 410 identification of functional balance problems with impact in
 411 day-to-day living, that can be used to tailor balance interven-
 412 tions. Consequently, further developments should address
 413 any simulation incongruencies, which are essential to under-
 414 stand to which extent our VR Bus simulation is similar and
 415 representative of the actual functional ADL, and as such,
 416 the behaviour of our participants can be representative of it.

417 Concerning our crucial goal to assess the feasibility of
 418 such a VR-based simulation of a relevant ADL, we found
 419 relevant and promising results for assessing balance con-
 420 trol, from a dynamic posturography standpoint. Participants
 421 behaved differently and coherently when subjected to spe-
 422 cific variations of the visual stimuli; when the bus turned,
 423 participants responded significantly by adopting anticipatory
 424 postural adjustments in the medial–lateral axis. This sug-
 425 gests that the VR test can be used to trigger some anticipa-
 426 tory balance control responses successfully and therefore a
 427 useful tool to study balance control.

428 An analysis of participants' behaviour during the different
 429 trajectories of the VR bus ride showed significant correla-
 430 tions with selected measurements of the WBB-based pos-
 431 turography system (Llorens et al. 2016). Participants that
 432 were more successful in keeping their excursion low (in both
 433 axis) when fixating a static target during the posturography
 434 assessment had higher medial–lateral excursions when the
 435 VR ride presented them with increased contrary visual and
 436 vestibular information. In opposition, people who failed to
 437 be misled into a visual perturbation response had higher
 438 excursions when evaluated in ideal conditions. This finding
 439 suggests that the VR Bus Assessment of Balance tool is
 440 sensitive to detect people who have a low weight for visual
 441 information when integrating it along with somatosensory
 442 and vestibular information for balance and postural control.

443 These results support our proposed paradigm's feasibility
 444 based on a more ecologically valid scenario in the context
 445 of a meaningful daily living activity. However, the fact that

446 most responses observed during the VR bus ride were in
 447 the medial–lateral axis, and only turns elicited significant
 448 responses, revealed the inability of our system to trigger
 449 or measure significant anticipatory reactions in the anter-
 450 ior–posterior axis. This can have three explanations: while
 451 the amount of perceived motion during turns was enough,
 452 the optical flow created in straight segments was not. If this
 453 is the case, the simulation can be adjusted by increasing lin-
 454 ear acceleration values, narrowing the roads, or lowering the
 455 bus. Another alternative is that we did not measure the pos-
 456 tural adaptations; in this case, other posturography metrics
 457 should be investigated, such as the 25 joint's kinematic data
 458 collected by the Kinect v2. Lastly, there is also the unlikely
 459 possibility that this visual stimulus is simply not used for
 460 anticipatory adjustments.

5 Limitations and future work 461

462 While we obtained promising preliminary results, some
 463 limitations must be considered. First, by diverging from the
 464 abstract test approach and pursuing an ecologically valid test
 465 scenario we give the participants freedom to behave natu-
 466 rally. In our study, the participants were free to look around;
 467 this freedom certainly had consequences on our results, as
 468 head movement can lead to changes in the centre of pressure
 469 position. However, limiting head movements would have had
 470 an impact on postural control, as it is triggered by the ves-
 471 tibular system in automated responses to compensate for
 472 perturbation (Allum et al. 1997).

473 Second, our system is only able to provide visual and
 474 audio cues, and it does not afford physical accelerations or
 475 cues to the user's vestibular and proprioceptive systems.
 476 Because of this, the results we obtained from the visual
 477 turns of the bus cannot be expected to match a real bus ride
 478 response of participants, as they are, at most, anticipatory
 479 adjustments. Therefore, the lack of a compensatory postural
 480 adjustment trigger is the greatest obstacle to ecological
 481 validity of the system. While the present system provides
 482 highly ecological visual input, future developments should
 483 focus on adding motion and pressure-sensitive handholds to
 484 test ecological validity further. Also, future results should
 485 be compared to CoP displacements during real bus rides.

486 Third, though we aimed to provide an ecologically valid
 487 experience through a visual simulation of a bus ride, we have
 488 no evidence that if the visual stimulation of the virtual city
 489 was replaced by abstract imagery (keeping the same vec-
 490 tion), the results would differ. This should be tested as well.

491 Lastly, as this study was performed with healthy young
 492 adults, we cannot expect the results to be generalized to
 493 other populations. However, this feasibility study results
 494 encouraged us to follow up with a system re-evaluation in

495 assessing its discriminative properties in older adults with
496 an increased risk of falls, which is the system's real goal.

497

498 **Author's contributions** All authors contributed to the study concep-
499 tion and design. Maria Fernanda Montoya and Afonso Gonçalves did
500 material preparation. Data collection and analysis were performed
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512 **Availability of data and material** The anonymous data used
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514

515 Declarations

516 **Conflict of interest** The authors declare that they have no conflict of
517 interest.

518 **Code availability** The custom software used in this study is not yet
519 available but will be made available in the future.

520 **Informed consent** All participants in the study provided their written
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